Evaluation of the Ciba Corning Biotrack 512 coagulation monitor for the control of oral anticoagulation

I Jennings, R J Luddington, T Baglin

Abstract

The Ciba Corning Biotrack 512 coagulation monitor requires a minimal degree of technical expertise to operate, and is already in use for near-patient testing. This study evaluated the monitor for possible use in decentralised control of oral anticoagulant treatment. The monitor compared well with Manchester Reagent, suggesting that it could be used in areas where this thromboplastin is used for centralised control.

The inability of the monitor to allow for locally determined geometric mean normal prothrombin times in the calculation of the International Normalised Ratio (INR), and possibly the high International Sensitivity Index (ISI) of the thromboplastin used with the monitor, resulted in poor comparability with some other thromboplastins, particularly Thrombotest. These problems need to be addressed if the monitor is to be used for decentralised anticoagulant control.

Decentralised or “bedside” testing is being increasingly used to obtain rapid test results in several hospital departments, such as intensive care units and operating theatres. Such testing is also applicable outside hospitals in community health centres—for example, pregnancy testing and the monitoring of blood sugar in diabetes. With detailed guidelines recently published on the control and recommended doses of oral anticoagulants, coagulation testing and control of oral anticoagulant treatment could be carried out by general practitioners. This would relieve the increasing workload experienced by hospital laboratories. In this department the annual number of outpatient tests performed for oral anticoagulant control increased by over 40% since 1987 to almost 10 000 tests a year. It could also lead to major financial savings in costs incurred from transporting samples or indeed patients from the community to hospital anticoagulant clinics. This approach requires a method for anticoagulant control which satisfies the criteria for decentralised testing—namely, the rapid production of results which can be accurately and reliably obtained by staff with a minimum of training and laboratory experience.

The Ciba Corning Biotrack 512 coagulation monitor is an automated technique for whole blood measurement of the prothrombin time, using capillary blood sampling. It is already used in operating theatres for preoperative monitoring of coagulation during liver transplantation, and a similar model, the Protrack Monitor 1000, correlates well with reference prothrombin time methods, both for normal subjects and patients receiving anticoagulation. This monitor has also been used for patient self-management of oral anticoagulant control in the United States.

In this study the 512 monitor was used in a series of outpatient anticoagulant clinics in parallel with the existing method of anticoagulant control, the Nycomed capillary thrombotest reagent, to compare the international normalised ratios (INRs) obtained by each method. Subsequently, the performance of the 512 monitor was compared with several different commercial thromboplastins.

Methods

INRs were measured on 104 patients receiving warfarin for a variety of conditions, and 20 normal subjects. Capillary blood was obtained from a fingerprick sample. Venous blood was collected into a 1/10th volume of 3.8% trisodium citrate, centrifuged at 2500 × g for five minutes, and separated into plastic tubes before the plasma INRs were measured.

Measurement of the prothrombin time by the 512 monitor was as follows: a prothrombin time cartridge, consisting of a capillary channel leading into a chamber containing dried thromboplastin (Ciba Corning, Halstead, Essex: batch P80236) was inserted into the monitor to warm to 37°C. A drop of capillary blood was added to the sample application well. The blood was drawn by capillary action into the monitor where it rehydrated the thromboplastin reagent. As clot formation occurred, capillary blood flow ceased, and this was detected by variation in light scatter of the red blood cells. The monitor then displayed both the prothrombin time and an INR calculated from stored values for the mean normal prothrombin time and the ISI of the thromboplastin reagent used.

Capillary thrombotest was carried out on the same fingerprick sample. Blood (50 µl) was aspirated and added to 250 µl of capillary thrombotest reagent (Nycomed, Oslo Norway; batch 003002) at 37°C. The clotting end point...
was measured manually by tilt-tube technique. The INR was calculated from the manufacturer’s chart.

Plasma INRs were determined with different thromboplastins on a KC10 coagulometer (Baxter Dade, Dudingen, Switzerland) as the determination of INR from clotting times obtained with this coagulometer has been shown to compare closely with manual methods.7 The following techniques were used: For Thromboplastin-1S (Baxter; Dade; batch 515-014), Simplastin (Organon Teknika, Boxtel, Holland; batch 10126750), and PT-Fib reagent (Instrumentation laboratories, Ascoli Piceno, Italy; batch 10500149), 0-1 ml plasma was added to a sample cuvette. Pre-warmed thromboplastin (0-2 ml) was added to the sample and the prothrombin time determined. For Manchester reagent (Manchester Thrombosis Research Foundation, Stockport), 0-1 ml plasma was added to the sample cuvette, followed by 0-1 ml thromboplastin. Finally, 0-1 ml 0-025 M calcium chloride was added, and the clotting time measured.

For venous thrombostest 0-03 ml plasma was added to 0-25 ml venous thrombostest reagent (Nycomed; batch 003002, reconstituted in 3-2 mM calcium chloride) and the clotting time was measured.

The INRs displayed by the 512 monitor were automatically calculated, based on a stored mean normal prothrombin time of 12 seconds and an ISI recorded on the test cartridge.

Capillary and venous thrombostest INRs were determined from the manufacturer’s chart. For all thromboplastins, including the 512 monitor and thrombostest reagent, the INR was also calculated by the UK NEQAS recommended method (Steering Committee letter to participants, June 1989) from the equation:

\[
\text{INR} = \frac{\text{PT patient}}{\text{geometric mean normal PT}} \times \text{ISI}
\]

where the mean normal PT was calculated as the geometric mean of the prothrombin times of 20 normal subjects (GMNPT), and the ISI was provided by the manufacturer.

A "consensus" INR was calculated as the mean INR for each sample derived from all methods.

Precision was assessed by determining the coefficients of variation (CV) for low and high INR control preparations obtained from the manufacturer. The CVs were calculated from the standard deviation/mean of 20 samples of each control.

The correlation coefficient is a measure of relation and not agreement between assays measuring the same parameter; calculation of the mean difference between assay measurements and the standard deviation of this mean is a more appropriate measure of agreement. Therefore, statistical evaluation was carried out by analysis of method of comparison, as described by Bland and Altman.8 The mean difference between individual patient INRs measured by different thromboplastins was calculated, and the standard deviation of this mean was used to obtain limits of agreement—that is the potential variation in an individual measurement, when using different thromboplastins. Thromboplastins giving a positive mean difference show a relative tendency to overestimate the degree of anticoagulation. Conversely, a negative mean difference indicates a relative tendency to underestimate the INR.

Results

Precision

Coefficients of variation measured for the control preparations on the 512 monitor were mean INR 0-79, CV 7-5%, and mean INR 4-3, CV 4-5%.

Comparability

INRs on 104 anticoagulated patients were measured using the 512 monitor and capillary thrombotest reagent. The calculated INR from the 512 monitor and the INR determined from the manufacturer’s chart for thrombotest reagent were compared. Results are shown in table 1 and the mean difference and limits of agreement are shown in figure 1. These show a significant underestimation of the INR by the 512 monitor relative to capillary thrombotest, and a potential difference in an individual INR measurement of up to 2-17 INR units.

The GMNPTs for the 512 monitor, capillary and venous thrombostest, and for four other thromboplastins are shown in table 2, together with the manufacturers’ ISI for each method.

The mean difference from the consensus INR and the limits of agreement for each thromboplastin are shown in table 3. The greatest difference from the consensus INR was

<table>
<thead>
<tr>
<th>Table 1</th>
<th>Comparison of INR results from 512 monitor and capillary thrombotest</th>
</tr>
</thead>
<tbody>
<tr>
<td>512 INR</td>
<td>Capillary thrombotest</td>
</tr>
<tr>
<td>Mean INR</td>
<td>2.44</td>
</tr>
<tr>
<td>Median INR</td>
<td>2.39</td>
</tr>
<tr>
<td>Minimum</td>
<td>0.89</td>
</tr>
<tr>
<td>Maximum</td>
<td>5.97</td>
</tr>
<tr>
<td>Range</td>
<td>5.08</td>
</tr>
</tbody>
</table>

* p < 0.001 (student’s t test).

Figure 1 Comparison of 512 monitor and capillary thrombotest. The tendency of the 512 monitor to underestimate the relative INR is shown by the mean difference of −0.76.
The thromboplastin-IS reagent consisted of a mean normal prothrombin time for all thromboplastins of 0.09.

The mean (SD) difference (reagent-consensus) was -0.05 (0.30) for 512 INR, 0.06 (0.30) for GMNPT INR, 0.24 (0.36) for Capillary thrombotest, 0.11 (0.33) for GMNPT INR, 0.03 (0.33) for Venous thrombotest, 0.11 (0.33) for GMNPT INR, 0.06 (0.32) for Thromboplastin-1S, 0.22 (0.36) for PT-Fib, 0.22 (0.36) for Simplastin, and 0.25 (0.35) for Manchester Reagent.

The limits of agreement indicated that the INR obtained from the 512 and the capillary thrombotest reagent may differ by up to 2.1 INR units (mean difference + 3SD). As both different Methods and different thromboplastins were used in deriving these INRs the performance of the 512 coagulometer and four thromboplastins, together with venous and capillary thrombotest, were evaluated. For each reagent (including the 512) the mean difference from consensus INR was calculated. Four of the 10 methods (including thrombotest) tended to overestimate the INR compared with the consensus, while six (including the 512) tended to underestimate the INR compared with the consensus. The thromboplastins most comparable with the 512 were Manchester Reagent and Simplastin. When the monitor INRs were compared with Manchester Reagent alone there was close comparability (mean difference -0.07). Thus in this study the 512 INR is most comparable with the Manchester Reagent INR and least comparable with the thrombotest INR. When the 512 INR was derived from the GMNPT it was comparable with the consensus INR (mean difference -0.09). There is no facility within the monitor, however, to change the calculation of the INR, necessitating manual calculation which complicates what would otherwise be a simple to read measurement of anticoagulation.

The limits of agreement between the consensus INR and the different thromboplastins ranged from -1.35 to 1.16, indicating that an INR can differ from the consensus by more than the full therapeutic range of anticoagulation (2.0 to 3.0 by BSH criteria) depending on the thromboplastin. The greatest limit was 1.35 INR units from the consensus INR in the case of the 512 INR. When the 512 INR was calculated from the GMNPT the mean difference from the consensus INR was minimal and the greatest limit from the consensus mean was reduced to 1.09. This wide limit of agreement might be expected as the ISI for the thromboplastin reagent was calculated as 2.07, which as a particularly high ISI may result in poor coefficients of variation and precision of results.8 The precision of the instrument, however, was shown to be good for both low and high INR values, with coefficients of variation of 7.5% or less. The wide limit of agreement is therefore not readily explicable.

Table 2  ISI and mean normal prothrombin time for all thromboplastins

<table>
<thead>
<tr>
<th>Thromboplastin reagent</th>
<th>ISI</th>
<th>Geometric mean (n = 20)</th>
</tr>
</thead>
<tbody>
<tr>
<td>512: Machine-calculated INR</td>
<td>2.07</td>
<td>12.00*</td>
</tr>
<tr>
<td>GMNPT-calculated INR</td>
<td>2.07</td>
<td>11.45</td>
</tr>
<tr>
<td>Capillary thrombotest</td>
<td>0.96</td>
<td>33.50</td>
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<tr>
<td>Capillary thrombotest:</td>
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<td></td>
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<tr>
<td>GMNPT-calculated INR</td>
<td>0.96</td>
<td>34.90</td>
</tr>
<tr>
<td>Venous thrombotest</td>
<td>0.98</td>
<td>34.50</td>
</tr>
<tr>
<td>Venous thrombotest:</td>
<td></td>
<td></td>
</tr>
<tr>
<td>GMNPT-calculated INR</td>
<td>0.98</td>
<td>35.16</td>
</tr>
<tr>
<td>Thromboplastin-1S</td>
<td>1.24</td>
<td>14.00</td>
</tr>
<tr>
<td>PT-Fib Reagent</td>
<td>1.37</td>
<td>15.48</td>
</tr>
<tr>
<td>Simplastin</td>
<td>1.23</td>
<td>13.58</td>
</tr>
<tr>
<td>Manchester Reagent</td>
<td>1.09</td>
<td>13.98</td>
</tr>
</tbody>
</table>

*Pre-determined by manufacturer.
+From manufacturer’s chart.
JISIs determined for manual and Automated Coagulation Laboratory (ACL) methods; manual ISI used.

Discussion

The first stage in evaluation of any new technique for decentralised testing is full evaluation of that technique by trained laboratory staff, and comparison with existing, quality controlled methods. The 512 monitor was easy to use, requiring no expertise and minimal training. Variables such as temperature control, subjective end point analysis, and accurate measurement of blood and reagent volumes have been removed, so that with adequate quality control, the instrument should prove suitable for decentralised testing.

The initial comparison between INRs obtained from the 512 monitor and capillary thrombotest showed poor comparability, with the 512 underestimating the INR by a mean of 0.76 INR units relative to the thrombotest reagent. The limits of agreement indicated that

![Figure 2 Comparison of 512 monitor and Manchester Reagent, showing close comparability of methods.](http://jcp.bmj.com/ on October 29, 2017 - Published by group.bmj.com)
but may result from the monitor under-estimating high INR values (INR > 4.0). This seemed to be a tendency with the machine, but the number of patients falling within this range was small and this could not be shown statistically.

In conclusion, the 512 monitor may be a suitable instrument for decentralised anticoagulant control as it is easy to use and precise. It would be particularly applicable for use in areas where centralised control is carried out using a similarly performing thromboplastin, such as Manchester Reagent. In its present form it would not be applicable in areas with centralised control using thromboplastins such as thrombostest. The latter incompatibility might be reduced if the facility for changing the GMNPT were introduced, but close compatibility with thromboplastins such as thrombotest would probably require a change of the thromboplastin incorporated in the 512 coagulometer. These factors need to be considered if the monitor is to be critically evaluated for decentralised control of oral anticoagulation.

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